Effects of train noise and vibration on human heart rate during sleep: an experimental study

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ABSTRACT

Objectives: Transportation of goods on railways is increasing and the majority of the increased numbers of freight trains run during the night. Transportation noise has adverse effects on sleep structure, affects the heart rate (HR) during sleep and may be linked to cardiovascular disease. Freight trains also generate vibration and little is known regarding the impact of vibration on human sleep. A laboratory study was conducted to examine how a realistic nocturnal railway traffic scenario influences HR during sleep.

Design: Case-control.

Setting: Healthy participants.

Participants: 24 healthy volunteers (11 men, 13 women, 19–28 years) spent six consecutive nights in the sleep laboratory.

Interventions: All participants slept during one habituation night, one control and four experimental nights in which train noise and vibration were reproduced. In the experimental nights, 20 or 36 trains with low-vibration or high-vibration characteristics were presented.

Primary and secondary outcome measures: Polysomnographical data and ECG were recorded.

Results: The train exposure led to a significant change of HR within 1 min of exposure onset (p=0.002), characterised by an initial and a delayed increase of HR. The high-vibration condition provoked an average increase of at least 3 bpm per train in 79% of the participants. Cardiac responses were in general higher in the high-vibration condition than in the low-vibration condition (p=0.006). No significant effect of noise sensitivity and gender was revealed, although there was a tendency for men to exhibit stronger HR acceleration than women.

Conclusions: Freight trains provoke HR accelerations during sleep, and the vibration characteristics of the trains are of special importance. In the long term, this may affect cardiovascular functioning of persons living close to railways.

INTRODUCTION

As the European market share of freight traffic is expected to increase from 8% in 2001 to 15% in 2020,1 it is important to estimate the impact this may have on the health of persons living close by to railway lines. Railway noise is related to disturbed sleep,2–6 which in turn increases the risk of cardiovascular disease,7 supported by indications of increased cardiovascular disease in persons living close to railways.8 Understanding how railway noise and vibration influence the cardiovascular system in sleep is therefore necessary.

The sympathetic tone is reduced in sleep, which is reflected by a reduction of heart rate (HR).9 External noise events have the potential to disturb sleep and lead to event-related increase of HR. This has been shown for pure tones10 and more recently for traffic noise.11 12 Noise-induced HR changes do not seem to habituate during sleep,12 therefore, they might ‘bear a pathogenic potential for the genesis of cardiovascular disease’.11 Evidence that long-term traffic exposure can increase the risk for cardiovascular disease comes from field studies.
Babisch summarises that traffic exposure enhances the risk for hypertension by a factor of between 1.5 and 3.14. An increased risk for myocardial infarction in persons living close to roads and railways has been found in several studies,15–18 although the effect sizes are rather small and the effects seem to be more pronounced in men.15 16 18

Traffic noise influences sleeping structure19 and leads to increased awakenings20 throughout the night. People living close to busy roads and railways or in close proximity to airports therefore often report poor sleep quality.3 4 6 A Dutch study revealed that the number of people reporting strong difficulties falling asleep due to traffic noise increased from 18% to 23% between 1998 and 2003.21 Disturbed sleep might be one factor leading to enhanced cardiovascular risk in persons exposed to traffic. It has been suggested that sleep disturbances contribute to cardiovascular disease through the pathway of enhanced inflammatory processes22 or, related to this, through the pathway of enhanced stress reaction affecting the cardiovascular system.23 In a field study, Carter et al24 examined the influence of nocturnal traffic exposure on seven older men with cardiac arrhythmia, who lived close to a busy road. They found an increased likelihood of single ventricular premature contractions (a form of cardiac arrhythmia) after noise peaks.

Two environmental exposures commonly arising from traffic are noise and vibration. As described, traffic noise disturbs sleep and leads to event-related HR changes, but the effect of traffic vibration is not well understood. Studies investigating annoyance show that (1) traffic vibration causes annoyance, (2) annoyance increases with increasing vibration level and (3) vibration enhances the annoying effect of noise.25–27 Furthermore, higher vibration amplitude is related to higher reported sleep disturbances in persons exposed to railway traffic.6 A study on human fetuses suggests that short experimental external vibration exposure alters sleep stage.28 Indications that vibration exposure is disadvantageous for cardiovascular function have been found in people exposed to high levels of vibration at work.29 30

The effect of combined traffic vibration and noise on the cardiovascular system in sleep has not been examined, to the best of our knowledge. It is the aim of the present study to detect if nocturnal noise and vibration exposure from freight trains provoke HR accelerations.

**METHODS**

**Participants and procedure**

Twenty-four volunteers (11 men, 13 women, 19–28 years, mean age 22.9 ± 2.8 years) slept in our sleep laboratory. Twenty-three were students and one was in full-time employment, recruited by public advertisements placed around the campus of the University of Gothenburg. Eligible persons were required to be aged between 18 and 30 years, in healthy condition, maintain normal sleeping patterns and not use tobacco products. To decrease the probability of subclinical breathing difficulties or apnoea, participants were required to have a body mass index within the normal range 18.5–24.99.31 Following initial screening, hearing was tested before volunteers were accepted. Manual audiometric testing was conducted using an Entomed SA2011 according to ISO 8253–1. Left and right ears were tested separately at frequencies of 250, 500, 1000, 2000, 3000, 4000, 6000 and 8000 Hz with hearing considered to be normal if measured thresholds were not more than a screening level of 20 dB HL.

The participants were instructed to begin attempting to fall asleep at 23:00 each night, were awoken by an alarm call at 07:00 each morning, and were prohibited from sleeping outside of this period. Before attending, they were asked about their noise sensitivity on a 5-point Likert scale. Fourteen participants (8 men and 6 women) rated themselves as being noise insensitive (points 1–2) and 10 rated themselves as being noise sensitive (points 3–5). For each participant, the study consisted of one habituation night and one control night preceding four experimental nights in which simulated trains passed. The arrangement of the experimental nights was randomised across participants. Gender and noise sensitivity was approximately equally spread around the randomisation table. In two of the four experimental nights, the participants were exposed to 20 trains per night with all trains having high vibration on one night and low vibration on the other night (High20 and Low20, respectively). On the remaining two nights, they were exposed to 36 trains per night, again with either high or low vibrations (High36 and Low36). The acoustic signal for the trains was not varied with vibration amplitude. There were more train passages between the periods of 23:00–01:00 and 05:00–07:00 to reflect typical real-world scenarios.

The sleep laboratory consists of three individual rooms isolated from external noise and vibration, furnished to simulate a typical bedroom with a bed, chairs, a desk and a small chest of drawers. Eighty-eight ceiling loudspeakers reproduced the low-frequency content of noise below 125 Hz, and higher frequencies were generated by two loudspeaker cabinets in the room corners. Because of the unrealistically low background noise levels in the rooms (<14 dBA), for the duration of the trial, artificial ventilation noise was introduced at a level of 25 dBA measured at the pillow position on the bed. In addition to the bedrooms, the participants had private access to a shared communal space outfitted with a kitchen, dining area and living area with a sofa and television. They were free to come and go as they desired during the daytime, being required to arrive by 20:00 each evening to ensure rest prior to bedtime and to allow sufficient time for electrode attachment.

Vibration and noise exposure were similar to that in another study conducted in our laboratory32 and are only summarised here. Five different train passages were
synthesised based upon analysis of the accelerometer and sound level measurements performed in the field. Noise signals were low pass filtered to correspond to a fully closed window. The vibration exposure was an amplitude-modulated 10 Hz signal applied along the lengthwise horizontal axis of the bed by electrodynamic shakers with a frequency response of 5–40 Hz mounted to the underside of the bed frame. The vibration began when the train noise signal exceeded an A-weighted equivalent level (L_{Aeq}) of 35 dB, ensuring masking of any audible mechanical operation noise. Further acoustic and vibration data for each individual train are presented in table 1.

Cardiac response and polysomnography
During all experimental nights, physiological data were recorded using ambulatory polysomnogram devices (SOMNOscreen plus PSG+, SOMNOmedics GmbH, Germany). The time resolution of the onset was 4.7 ±3.4 s.

Cardiac activity was recorded via a modified lead II torso placement ECG at a sampling frequency of 256 Hz as per the American Academy of Sleep Medicine.33 To identify sleep stage, EEG, electrooculogram and submental electromyogram were also recorded using standardised surface electrode placements and sampling and filter frequencies. To ensure good signal quality, following electrode attachment it was checked that the electrical impedance of each contact was ≤5 kΩ. Thirty second epoch sleep staging was performed manually by a trained sleep technician. Additionally, participants wore two effort belts to record breathing rates and a finger pulse oximeter to record blood oxygen saturation, plethysmogram and pulse information, although these data will not be reported here. Owing to a technical fault, ECG was not obtained for one participant (female, noise sensitive) in the High20 night and therefore could not be included in analysis.

Event-related analysis and control condition
In order to examine event-related changes of HR, data from the four exposure nights were analysed. The continuously recorded ECG (sampling frequency of 256 Hz) was converted into HR (in bpm) in 1 s intervals through the whole night. EEG and ECG recordings were synchronised with the train exposure events, thus allowing a direct temporal association between the occurrence of a train and the participant’s HR reaction and sleep stages. Analysis revealed that 9.9% of the train onsets occurred during wake stage, 8.1% during stage N1, 42% during stage N2, 21.4% during stage N3 and 17.8% during rapid eye movement (REM).

The procedure of HR analysis is visualised in figure 1. HRs below 35 and above 130 bpm were excluded from the analysis.11 This was the case for 4.1% of the events. For analysis of event-related HR change (bpm), only train events where participants were asleep were considered. This approach was chosen because Griefahn et al.11 showed that HR response to traffic noise differs depending on whether the participants do or do not awake. The relatively few trains per night in our study do not allow additional examination of HR response in the case of awakenings. An event-related awakening has been defined as a sleep stage change to Wake from any other stage in at least one of the two epochs (30 s) following the train onset.35 The first of these was determined by that having at least 15 s under influence of the event. Additionally, events for which the participants were awake in the epoch preceding train onset were excluded from the analysis. The whole procedure left 72.4% of the train events in the low-vibration condition and 66.1% of the train events in the high-vibration condition for analysis. In accordance with the literature, the screening interval for cardiac activations was set to 60 s after train onset.11 In order to analyse change of HR, the average cardiac response from the 10 s preceding the train event was used as a baseline value for each given event and subsequently subtracted from the cardiac response in each of the 60 s time intervals following the train onset.

In order to examine if there was a train-related change of HR at all, ‘fake trains’ were calculated. Fake trains were defined as time intervals of 60 s not accompanied by a real train event, distributed at time intervals equally spaced between the actual exposure events. Twenty of these were introduced in the Low20...
and High20 nights and 36 in the Low36 and High36 nights. Analysed HR data for these consisted of 70 s, where 10 s served as baseline for the following 60 s. As with the real exposures, data where polysomnographical analysis indicated that participants were awake before onset or awoke during the two epochs following onset were excluded. All event-related 60 s periods were subsequently averaged over nights with low or high vibration, respectively. The whole procedure was the same for each of the four nights to avoid any potential investigator bias.

Griefahn et al\(^1\) report a maximum increase of HR about 13.2 s after event onset. We took this time interval ± 3 s as a base for the searching area for the maximum increase between 10 and 16 s after train onset.

**Statistical analysis**

Data were analysed using SPSS V20 (SPSS Inc, Illinois, USA). In order to identify any overall effect of trains on HR, the integral of the HR response was taken to determine the area under the curve (AuC) for the 60 s after train onset. An analysis of variance (ANOVA) for repeated measurements was calculated comparing AuC in three factors: event (fake vs real-train), vibration level (low vs high) and number of trains (20 vs 36). The effects of noise sensitivity and gender were also analysed using ANOVA for repeated measurements with the between-subject factor noise sensitivity/gender and the within-subject factor vibration level (low vs high). Post hoc comparisons are reported Bonferroni-corrected. The level of significance is set at \(\alpha=0.05\).

**RESULTS**

**Influence of train noise and vibration on HR**

The AuC analysis for the change of HR 60 s after event onset revealed a significant main effect of the train, indicating that train events lead to an enhanced change of HR compared with the fake events (\(F_{22,1}=12.0, p=0.002\)). Furthermore, there were significantly more awakenings in the train vs fake events (\(F_{22,1}=40.3, p<0.001\)).

There was a significant main effect of vibration level. A higher change of HR and an increased number of awakenings could be observed in the high vibration level compared to the low-vibration level (HR: \(F_{22,1}=7.6; p=0.01\); awakenings: \(F_{22,1}=6.5; p=0.014\)). The number of trains had no significant influence on the HR change. The results are displayed in table 2.

Averaged over all trains within one night, an increase of HR of at least 3 bpm was observed in 54% of the participants in Low36, 52% in the Low20 condition, 74% in the High20 night and 79% of participants in the High36 night. For the fake train events, an average increase of HR of at least 3 bpm was observed in only 17–38% of the participants, depending on the exposure night.

As no significant influence of the number of trains was revealed, the four exposure conditions were combined into two conditions: a high-vibration condition and a low-vibration condition. This approach is advantageous for the signal–noise ratio, because in this way the number of analysable trains could be increased to 56. For calculating the low-vibration condition, train events from the Low20 and Low36 nights that matched the
inclusion criteria described in the methods section were averaged to obtain one low-vibration response. The same method was performed for the high-vibration condition. This procedure was repeated for the fake events, so that the resulting responses for the low-vibration and high-vibration exposures for both the actual and phantom events could be compared.

Characteristics of the HR curve

The HR curve shows a biphasic characteristic (see figure 2A). After approximately 9 s, a short initial response characterised by increase of HR takes place, lasting for around 6 s. This initial response is significantly above the baseline between 10 and 13 s for the low-vibration condition, and between 10 and 15 s for the high-vibration condition (t test, p<0.05). This response is in accordance with the proposed search area of the maximum increase.

An additional delayed response can also be observed. This response is characterised by a second increase of HR beginning around 17 s following train onset and with a duration of around 20 s for the low-vibration condition and about 30 s for the high-vibration condition. The delayed response is significantly above the baseline between 21 and 22 s for the low-vibration condition, and between 20 and 48 s for the high-vibration condition (t test, p<0.05). This same response could be seen for each of the five individual train types (see figure 2B)

### Table 2  Analysis of event-related HR response for each of the four exposure nights and combined for low-vibration and high-vibration exposure

<table>
<thead>
<tr>
<th></th>
<th>Low vibration Mean (SD)</th>
<th>High vibration Mean (SD)</th>
</tr>
</thead>
<tbody>
<tr>
<td></td>
<td>20 Trains/night N=24</td>
<td>36 Trains/night N=23</td>
</tr>
<tr>
<td></td>
<td>20 Trains/night N=23</td>
<td>36 Trains/night N=24</td>
</tr>
<tr>
<td>HR AuC</td>
<td></td>
<td></td>
</tr>
<tr>
<td>Train</td>
<td>41.7 (114.5)</td>
<td>77.2 (103.0)</td>
</tr>
<tr>
<td>Fake</td>
<td>−4.6 (83.7)</td>
<td>0.2 (54.4)</td>
</tr>
<tr>
<td></td>
<td>19.4 (77.6)</td>
<td>−7.4 (51.5)</td>
</tr>
<tr>
<td></td>
<td>52.3 (86.8)</td>
<td>2.2 (60.9)</td>
</tr>
<tr>
<td>Number of event-related awakenings per night</td>
<td></td>
<td></td>
</tr>
<tr>
<td>Train</td>
<td>3.3 (2.3)</td>
<td>4.2 (2.6)</td>
</tr>
<tr>
<td>Fake</td>
<td>1.5 (0.7)</td>
<td>1.5 (0.6)</td>
</tr>
<tr>
<td>Event-related HR change of at least 3 bpm</td>
<td></td>
<td></td>
</tr>
<tr>
<td>Train</td>
<td>15 (62.5%)</td>
<td>17 (73.9%)</td>
</tr>
<tr>
<td>Fake</td>
<td>9 (37.5%)</td>
<td>8 (34.8%)</td>
</tr>
</tbody>
</table>
| Area under the curve (AuC), number of event-related awakenings, initial and delayed maximal increase of heart rate (HR) and number of participants with an event-related change of HR of at least 3 bpm are presented for each of the four experimental nights. AuC, initial and delayed maximal increase of HR are presented for the combined low-vibration and high-vibration conditions. Cave: the initial and delayed response is calculated as maximal increase within the first 10–15 or 20–48 s after train onset. This difference in search area explains part of the differences between the initial and delayed increase of HR.

This response pattern could be observed in the individual participants, but the time delay after event onset showed a great variability. The individual maximum for each participant within the range of the initial response (10–15 s) and the delayed response (17–50 s) was calculated and is reported in Table 2.

For the initial response and for the delayed response, ANOVA for repeated measurements revealed a significant main effect of the event, indicating that the train-events led to an enhanced change of HR compared with the fake-events (initial response: \(F_{23,1}=13, p=0.001\); delayed response: \(F_{23,1}=15.5, p=0.001\)).

The vibration level had no significant influence on the initial increase of HR (\(F_{23,1}=2.1, \text{n.s.}\)), but affected the delayed response. A higher delayed increase of HR was observed in the high vibration level compared to the low vibration level (\(F_{23,1}=9.4, p=0.006\)).

**Effect of order**

The participant’s HR responses of the four nights were compared with respect to the order of experimental nights using ANOVA for repeated measurements. There was no significant influence of order of experimental nights on the AuC response (\(F_{22,3}=1.7, \text{n.s.}\)), as well as for the initial (\(F_{22,3}=2.0, \text{n.s.}\)) or delayed response (\(F_{22,3}=0.8\)).

**Influence of sleep stage**

The AuC, the initial maxima and the delayed maxima were compared in the sleep stages N3, N2 and REM. For
the wake stage and for stage N1, there were too few events to allow for comparison. The results are presented in table 2.

ANOVA for repeated measurements using the within-subject factors sleep stage (stages N3, N2 and REM) and vibration level (low vs high) was calculated.

The overall AuC revealed no significant influence of sleep stage (F23,2=1.1, n.s.). The initial response revealed a significant influence of sleep stage (F23,2=5.1, p=0.009). Bonferroni-corrected post hoc comparison reveals that the initial increase of HR was significantly higher in REM than in stage N2 sleep (p=0.002). The same significant pattern was seen in the delayed response (F23,2=4.8, p=0.015). Here again, a post hoc comparison showed that HR increase was higher in REM sleep than in stage N2 (p=0.017).

**Influence of noise sensitivity and gender**

**Effect of sensitivity**

AuC, initial maxima and delayed maxima of HR change are compared between participants with low (N=14) and high (N=10) noise sensitivity. The results are displayed in table 3. No significant main effects of noise sensitivity were found in AuC (F22,1=0.007, n.s.) as well as in the initial (F22,1=2.8, n.s.) or delayed response (F22,1=0.004, n.s.). There were no significant interactions between noise sensitivity and vibration level.

**Effect of gender**

The results of comparisons between men (N=11) and women (N=13) are shown in table 3. No significant differences were found in AuC (F22,1=2.5, n.s.) or in the HR initial (F22,1=0.5, n.s.) between genders. There was a tendency for men to exhibit a stronger increase of HR in the delayed response (F22,1=4.1, p=0.055).

**DISCUSSION**

Our data show that train noise and vibration exposure lead to an increased number of awakenings and cardiac arousals, and that vibration might be of particular importance. HR acceleration with two maxima was observed following train noise and vibration. One rapid and distinct initial HR increase is evident around 9 s after train onset and a lengthier delayed increase is observed starting about 17 s after train onset. In a similar study dealing with traffic noise alone, Griefahn et al. found an increase of HR matching our initial response but no delayed increase. A similar initial increase of HR has been found for pure tones during sleep. Propose that the second plateau is due to the additional vibration exposure, which seems to either act in isolation to result in cardiac response, or alternatively enhance or interact with any delayed effects of rail noise on HR. Supporting this interpretation, we see a significant difference between the low-vibration and high-vibration levels for the delayed, but not for the initial increase. The combined exposure might be a more pronounced alarming signal than noise alone and the HR alterations endure even after cessation of the actual exposure. In accordance with the previous literature on sleep disturbance due to noise exposure, the highest alterations of HR were found in REM sleep. This was observed for both the initial and delayed response.

Cardiac arousals are very likely induced by brain stem activation. Subcortical activation may present a form of primary arousal in sleep and—depending on the strength of activation and on sleep stage—lead to cortical activation and arousal. Increased HR indicates subcortical arousal and enhances the probability of a cortical arousal with implications for sleep structure. However, even HR acceleration without concomitant cortical arousal has been shown to have adverse effects on sleep structure. Guilleminault et al. showed that forced subcortical arousals accompany disturbed sleep and the persons are not necessarily aware of their disturbed sleep the following morning.

In the short term, arousals have positive effects by ensuring a higher level of behavioural responsiveness in the presence of external stimuli, while sleep is protected as far as possible. However, in the long term, increased autonomic reaction might be harmful. As Kohler and Stradling point out in a review paper, recurrent arousals are one of the mechanisms leading to cardiovascular disease in obstructive sleep apnoea. In this manner, the autonomic arousals provoked by passing trains may—if continuing over a number of years —contribute to the slightly enhanced myocardial infarction risk that has been found in people living in areas with high traffic exposure. The study of Tassi et al. suggests that people living in areas with high railway noise for more than 10 years can partly adjust their sleep to this adverse exposure. However, even after such a long-term exposure, significant alterations of HR due to a nocturnal railway traffic scenario have been found. In epidemiological studies, the effects of noise exposure alone are rather small. Our data suggest that the effect of chronic traffic exposure on cardiovascular disease might be higher if vibration is additionally taken into account. As described in the methods of this paper, we excluded events from the analysis where the persons woke up. This approach allows a focused estimation of HR reaction from traffic noise during sleep. However, as HR reactions are usually greater if accompanied by awakenings, our results very likely underestimate the effects. We found an average train-related increase of 3 bpm in 79% of participants, supporting previously reported data. It is not possible with the present study design to estimate the clinical relevance of these results. However, an increase of HR in sleep perhaps reflects a higher sympathetic tone and this may contribute to the enhanced risk for hypertension in long-term traffic exposure.

Our results are less clear regarding the impact of interindividual differences. Previous epidemiological
research has shown that persons who state being sensitive to noise report greater sleeping problems due to traffic than non-sensitive persons. However, we found no significant effect of self-reported noise sensitivity on HR response towards nocturnal train events. During the day, it has been shown that self-declared highly noise sensitive persons have higher cardiovascular responses towards different ecologically relevant sounds, including traffic noise. The sample size of sensitive and non-sensitive participants in our study is relatively small, and therefore non-significant results in particular have to be interpreted with caution. The sample size also allows interpretation of gender effects. In coherence with the study of Griefahn, we found no significant gender differences in the initial HR amplitude. We found a tendency for enhanced delayed HR response in men with a rather strong effect size. This corresponds to results from several field studies, where enhanced traffic exposure related cardiovascular diseases were found in men.

We are aware of the limitations of the study: Regarding internal validity, the time resolution of the measurement could potentially lead to a smoothing of the averaged data, underestimating our results. Nevertheless, a clear effect of enhanced HR reaction in high vibration conditions can be seen. We argue that vibration exposure is responsible for the second plateau. However, a vibration-alone condition, that is, in the absence of noise, is needed to confirm this. With respect to external validity, the study is limited to the homogeneous group of young and healthy participants. To generalise the results, a broader age range would be preferable and the study should be replicated in field conditions.

In conclusion, the combined exposure of freight train noise and vibration influenced HR during sleep, whereby HR amplitudes increase with increasing vibration level. This provoked acceleration may affect cardiovascular function in the long term and could be a mechanism explaining the previous findings of cardiovascular disease in persons exposed to traffic in general and rail traffic in particular. To study the specific influence of vibration in contrast to noise, further studies are required.

Provenance and peer review Not commissioned; externally peer reviewed.

Data sharing statement No additional data are available.

REFERENCES


